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Understanding the encapsulation and release of small molecular weight model actives from alginate fluid gels

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11 Abstract

12 The inclusion of actives within a range of biopolymer-based formulated gelled systems has 13 been receiving significant attention. Among these, encapsulation in gelled microparticles has 14 generated substantial interest, but such systems still face challenges for scalable production. 15 Fluid gels are a class of soft-solid particles produced via high-shear approaches that are suitable 16 for industrial manufacture. However, their use for the entrapment of species of 17 therapeutic/nutritional activity has been scarcely investigated. The aim of this work was to 18 study the encapsulation/retention of different small molecular weight actives of varied 19 hydrophilicity/hydrophobicity within alginate fluid gels (AFG). The presence of an active 20 during AFG formation did not interfere with gel particle dimensions nor bulk rheological 21 behaviour. Following production, encapsulation of all actives within the fluid gel particles was 22 very low, but significantly increased for the hydrophobic ones with storage. The rate and extent 23 of hydrophobic active loading in the AFG particles were governed by the concentration of the 24 former and gel particle size. Release studies under sink conditions revealed that hydrophobic 25 active content within the AFG particles is not expelled and remains fully entrapped regardless of fluid gel particle size and storage period. A hypothesis suggesting that the loading of 26 27 hydrophobic actives within the AFG particles is due to changes to the solvent quality of water, 28 is presented. Overall, the current study offers insight into the use of alginate fluid gels as 29 encapsulation media and presents original findings that can greatly support future efforts to 30 expand the applicability of these industrially-relevant colloidal systems.

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32 Keywords: Alginate; Fluid gels; Encapsulation Efficiency; Release.

1 **1. Introduction**

2 Material and microstructures that can enable the controlled release of active ingredients 3 are increasingly used in both the foods and pharmaceutical industries. Microencapsulation 4 matrices, such as liposomes, microgels, emulsions and/or microemulsions, have been studied 5 for such purposes in foods (Ray et al., 2016). These formulations can be designed in order to 6 achieve different performances, such as to prolong the function of actives by delaying their 7 release, protect sensitive components from adverse environmental conditions (e.g. high 8 moisture content, acidity, presence of enzymes, etc.) and/or mask unwanted tastes (Wischke & 9 Schwendeman, 2008).

10 Amongst all such microstructures, hydrocolloid gel particles have received significant 11 research attention due to their biocompatibility (Burey et al., 2008). However, the majority of 12 current microencapsulation technologies based on hydrocolloid microparticles, face challenges 13 in terms of scalable production (Ozkan et al., 2019). Over the last two decades a new approach 14 for the production of biopolymer-based microparticles, commonly termed as sheared or fluid 15 gels, has been investigated (Norton et al., 1999; Shewan & Stokes, 2013). Fluid gels are 16 suspensions of gel particles in a non-gelled continuous medium, usually water, produced when 17 a biopolymer solution undergoes gelation whilst subjected to shear (García et al., 2018; Garrec 18 & Norton, 2012; Norton et al., 1999). Fluid gels can be produced continuously using typical 19 shear devices (e.g. pin-stirrer) and as such their scalable manufacture is less problematic 20 (Fernández Farrés et al., 2013). Because of their unique rheological properties/characteristics, 21 fluid gels have been mainly studied as texturing materials for applications in food products 22 (Chung et al., 2014; Fernández Farrés et al., 2014; Le Révérend et al., 2010; Norton et al., 23 2015). Tribological studies have also shown the ability of these systems to provide lubrication, 24 suggesting that they can impart an in-mouth sensory response similar to that typically 25 associated with fat (Fernández Farrés et al., 2014).

26 Despite their current applications, literature on the utilisation of fluid gels for entrapment 27 and delivery purposes is extremely scarce. The current authors used alginate fluid gels to study 28 the encapsulation of tryptophan and showed that overtime such matrices can slow down the 29 release of the active (Smaniotto et al., 2019). In another study, ter Horst et al. (2019) studied 30 the entrapment of skin cells in gellan gum fluid gel systems in order to enable their delivery 31 onto burn wounds. The authors reported that cell viability was not compromised by 32 encapsulation in the gellan fluid gels nor by the subsequent spray application (ter Horst et al., 33 2019). Nonetheless, the mechanism for the encapsulation of actives within fluid gel formulations is far from understood, while key parameters that can affect both encapsulation
 as well as subsequent release (for example, the influence of gel particle size), have simply not
 been investigated.

4 The present work aims to understand the encapsulation and release of small molecular 5 weight actives from alginate fluid gel (AFG) formulations, as a function of the type (hydrophilicity/hydrophobicity) and concentration of the to-be-entrapped species and AFG 6 7 particle size. AFG formation was carried out within a pin-stirrer vessel both in the presence 8 and absence of the actives. In both cases, AFG particle size and bulk rheological behaviour 9 (shear viscosity) were measured. The encapsulation efficiency (EE) of all actives was 10 determined within 24 h of AFG production and then monitored over a period of 2 weeks 11 (following AFG production) during which all formulations were stored unperturbed at room temperature. The release of all actives from the AFG formulations was carried out under sink 12 13 conditions for both immediately produced and stored systems. The effect of AFG particle size 14 on the EE and release profiles for all (hydrophilic/hydrophobic) actives were studied. Overall, 15 the current study offers new insight into the use of AFG as encapsulation matrices in an attempt 16 to strengthen the industrial applicability of these colloidal systems.

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2. Materials and methods

19 2.1. Materials

20 Sodium alginate (ALG), vanillin (VAN, $\geq 97\%$), L-tryptophan (TRP, $\geq 98\%$ HPLC), and nicotinamide (NIC, ≥98%, HPLC), were purchased from Sigma-Aldrich[®] (UK). Calcium 21 22 chloride (CaCl₂, anhydrous, 93%) was purchased from Alfa AesarTM (USA). Vanillin and 23 tryptophan were chosen as hydrophobic actives, while nicotinamide as a hydrophilic one. All 24 material were used without further purification. Milli-Q distilled water, produced using an 25 Elix[®] 5 distillation apparatus (Millipore[®], USA), was used in all formulations. All 26 concentrations are given as % w/w; percentage of the weight of any specific compound over 27 the total weight of the system it is contained within (i.e. solution, fluid gel formulation).

28

29 2.2. Production of alginate fluid gels

30 2.2.1. Blank alginate fluid gels

The production of blank alginate fluid gels (AFG) follows the process used by Smaniotto *et al.* (2020). In brief, a 2% w/w alginate solution was prepared by dissolving the required amount of the compound in distilled water (95°C) under mild stirring for 45 min. An aqueous solution of CaCl₂ (0.25% or 0.35% w/w) was also prepared by dissolving CaCl₂ at room temperature under magnetic stirring. AFG were formed using a pin-stirrer device (Het Stempel, Netherlands), with an available processing volume of 150 mL, operating at a pin-shaft speed of 1000 rpm. The alginate solution was pumped into the pin-stirrer at 33 mL/min using a peristaltic pump (Masterflex L/S Peristaltic, Germany), while the CaCl₂ solution was injected into the pin-stirrer through a stainless steel needle (1.25 mm internal diameter) using a syringe pump (Cole-Parmer Single-syringe, USA) at 4.02 mL/min.

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9 2.2.2. Active-containing alginate fluid gels

10 Active-containing AFG were produced following a similar procedure. Each active 11 (0.05% or 0.10% w/w) was dissolved in distilled water at room temperature under magnetic 12 stirring, with CaCl₂ (0.25% or 0.35% w/w) then added to this. The alginate and active-13 containing CaCl₂ solutions were pumped into the pin-stirrer as above. Preliminary tests, where 14 the actives were incorporated within the alginate (rather than the CaCl₂) stream for entry into 15 the pin-stirrer, produced indistinguishable active-containing AFG formulations.

16

17 2.3. Rheological measurements

The shear viscosity of all blank and active-containing AFG formulations was measured using a rotational rheometer (KinexusTM, Malvern[®], UK) equipped with a 40 mm diameter sand blasted plate geometry. All analyses were carried out at 25°C using a shear rate ramp between 0.1 and 100 s⁻¹. All rheological measurements were carried out in triplicate and all shear viscosity data are presented/plotted as mean values \pm 1 standard deviation (SD). In order to assess bulk viscoelasticity, the shear viscosity profiles of all AFG formulations were fitted to a simple power-law model (Barnes *et al.*, 1989):

$$\eta = K_2 \dot{\gamma}^{n-1} \qquad \qquad \text{Eq. (1)}$$

25 where K is the consistency constant and n is the power-law index.

26

27 **2.4. Particle size analysis**

The particle size distributions (PSD) of all blank and active-containing AFG were evaluated using laser diffraction (Mastersizer-2000, Malvern[®], UK) and are presented as the numerical particle size percentage. Few drops of each fluid gel formulation were added to a pure aqueous phase contained within the chamber of the instrument where they were mixed at 1300 rpm for at least 10 min (necessary for a constant value of obscuration to be obtained) before performing the analysis. AFG particle dimensions previously determined using dynamic light scattering (Smaniotto *et al.*, 2020) were in agreement to the sizes measured here. Surface weighted mean diameters ($D_{3,2}$) and span values were provided by the Mastersizer-2000 software. All PSD measurements were carried out in triplicate and all $D_{3,2}$ and span data are presented/plotted as mean values ± 1 standard deviation (SD).

6 Selected AFG systems were also visualised using an optical microscope (DM 2500 LED, 7 Leica[®], CH) to, amongst others, confirm the particle size data obtained by laser diffraction. For 8 the purpose of this, AFG samples were firstly diluted with distilled water using a water-to-9 sample ratio of 10:1 and these were subsequently mixed using a vortex mixer (VM20, Rigal 10 Bennet[®], UK) for 20 seconds. Differential Interference Contrast (DIC) settings were set up to increase the contrast, allowing for clearer visualisation of the particles and their dimensions. 11 Images were captured using a CCD camera (DFC450C, Leica[®], CH) coupled to the microscope 12 (Figure 1). Image analysis to evaluate the dimensions of the microparticles was carried out 13 14 using the Leica Application Suite (LAS 4.8.0, Leica[®], CH). 15



Figure 1. Optical micrograph of AFG particles produced in a pin-stirrer device, using a 2% w/w and
 0.35% w/w alginate and CaCl₂ aqueous solutions, respectively.

19

20 2.5. Ultraviolet–visible (UV-Vis) spectroscopy

Ultraviolet–visible (UV-Vis) spectroscopy was used to determine the concentration of non-entrapped actives using the procedure employed by Smaniotto *et al.* (2019). In brief, the absorbance of all actives was measured at room temperature using an Orion AquaMate 8000 UV-Vis spectrophotometer (Thermo-Scientific[®], UK), at 300 nm for vanillin, 278 nm for tryptophan and 214 nm for nicotinamide. Absorbance was converted to concentration using the

- Beer-Lambert equation and correlation parameters obtained from active-specific calibration
 curves. All UV-Vis measurements were carried out in triplicate.
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4 **2.6. Encapsulation efficiency**

5 The encapsulation efficiency (EE) of all actives in the AFG particles was determined 6 following the procedure employed by Smaniotto *et al.* (2019). In brief, ~15g of fluid gel sample 7 were subjected to ultracentrifugation for 45 minutes, at 21°C and 21,000 rpm, using a Sigma 8 3K-30 refrigerated centrifuge (Sigma[®], Denmark), equipped with a 12150 rotor. A known 9 amount of the formed supernatant (~1.5 g) was placed in a 100 mL volumetric flask and filled 10 to full capacity with distilled water. The mass of the active in the supernatant was finally 11 determined via UV-Vis analysis. EE was then calculated as:

$$EE\% = \frac{W_i - W_t}{W_i} \times 100 \qquad \qquad Eq. (2)$$

12 where W_i is the amount of active initially added to the fluid gel formulation and W_t is the 13 amount of active in the supernatant (non-encapsulated active) of the same fluid gel formulation 14 at different time intervals *t*. The ($W_i - W_t$) difference therefore corresponds to the amount of 15 active that is encapsulated within the AFG particles (Piacentini, 2016).

16

17 **2.7. Release studies**

Approximately 2.5 g of an active-containing AFG formulation were enclosed in a dialysis 18 19 sack (cellulose dialysis tubing membrane, width 43 mm, MW cut-off of 14000 Da; Sigma-20 Aldrich, UK) which was then placed in 500 mL of distilled water (acceptor phase) at room 21 temperature (~ 21°C), under mild mixing provided by the use of a magnetic stirrer at 150 rpm. 22 At regular intervals, aliquots of 2 mL were withdrawn from the acceptor phase and measured 23 using UV-Vis spectroscopy to determine the concentration/amount of released active; 24 following their UV-Vis measurement, each withdrawn aliquot was added back into the acceptor 25 phase. All measurements were carried out in triplicate and all release data are presented/plotted 26 as mean values ± 1 standard deviation (SD). Release data were fitted to the Ritger-Peppas 27 model (Ritger & Peppas, 1987):

$$\frac{M_t}{M_{\infty}} = k_r t^{n_r} \qquad \text{Eq. (3)}$$

where M_t and M_{∞} are the cumulative amount of active released at time *t* and at infinite time (complete release), respectively, k_r is a kinetic constant, and n_r is the diffusional exponent characteristic of the release mechanism.

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2.8. Statistical analysis

2 All data are presented as mean values \pm one standard deviation (SD). Statistical 3 significance was determined by performing Student's t-test. Results were considered 4 statistically significant at *p*-values ≤ 0.05 .

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3. Results and discussion

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3.1. Effect of active type and concentration

9 Alginate fluid gels (AFG) were produced in the presence of actives and the effect of 10 active type (hydrophilic/hydrophobic) and concentration on AFG particle size (PSD), 11 rheological behaviour, encapsulation efficiency (EE) and release behaviour (under sink 12 conditions) were studied. Samples were produced by fixing the alginate and CaCl₂ concentrations at 2% w/w and 0.35% w/w, respectively. A previous study by the current 13 14 authors showed that, at these concentrations, AFG particles (no active present) in the size range 15 of 0.5-5 µm can be obtained (Smaniotto et al., 2020). The model actives used were selected 16 based on their water-solubility (hydrophilicity/hydrophobicity); vanillin and tryptophan were 17 chosen to represent low water-solubility actives (11 mg/mL and 13 mg/mL, respectively) and 18 nicotinamide to correspond to a model active of high water-solubility (500 mg/mL). Vanillin 19 is a natural flavour, tryptophan is an essential amino acid and nicotinamide is a form of vitamin 20 B₃ (Gibbs et al., 1999; Jelena et al., 2010). The concentrations of all actives tested here were 21 matched and kept below the aqueous saturation limit of the least water soluble one (i.e. 22 vanillin). As such, active concentrations of 0.05% to 0.10% w/w for VAN (VFG 0.05% and VFG 0.10%), TRP (TFG 0.05% and TFG 0.10%), and NIC (NFG 0.05% and NFG 0.10%) 23 24 were chosen.

25

26 3.1.1. Fluid gel particle size and rheological behaviour

27 All AFG produced in the presence of different actives were characterised in terms of 28 particle size (PSD) and bulk rheological behaviour (shear viscosity). Results were compared to 29 PSD and shear viscosity curves of blank AFG systems (formed in the absence of an active). 30 Size measurements, reported in Figure 2, revealed that all AFG formulations have practically 31 the same PSD, independently of the type and/or concentration of the active used. Blank and 32 active-containing AFG particles exhibited similar $D_{3,2}$ (1-3 µm) and span (1-2) values.



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Figure 2. Particle size distributions (A, B and C) and shear viscosity curves (D, E and F) for AFG formed in the absence (blank AFG) and the presence of different actives (vanillin, VFG; tryptophan, TFG; nicotinamide, NFG) as a function of active concentration (0.05% and 0.10% w/w). All data are given as mean values ± 1 SD (error bars).

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9 Shear viscosity profiles for all AFG formulations are also presented in Figure 1 together with 10 their fit to Eq. (1) and obtained model parameters. The shear viscosity curves for all systems 11 were comparable with similar K and n parameters; the latter also indicating that all formulations 12 exhibit a similar degree of shear thinning behaviour (Fox *et al.*, 2011). Overall, AFG particle 13 size and rheological performance does not appear to be affected by the presence or 1 concentration of either a hydrophilic or a hydrophobic active; at least within the range of 2 concentrations tested here. PSD and shear viscosity profiles, for all fluid gel systems, were 3 monitored over a period of 2 weeks following manufacture, and no significant deviation to 4 either of these parameters was observed (data not shown here).

5

6 3.1.2. Encapsulation efficiency

7 The data on the encapsulation efficiency (EE) for all active-containing AFG formulations 8 as a function of active type (hydrophilic/hydrophobic) and concentration are reported in Table 9 1. EEs were determined within 24 h of AFG production and then monitored over a period of 2 10 weeks, during which all formulations were stored unperturbed at room temperature; t_s is used 11 to denote the period under storage.

12

13 Table 1. Encapsulation efficiency (EE) in AFG formulations produced in the presence of different

actives (vanillin, VFG; tryptophan, TFG; nicotinamide, NFG), as a function of active type and 14 15 concentration, and storage time (t_s) . Differences between EE values (for the same active) marked with

16

the same superscripted letter are not statistically significant (p > 0.05).

Active-containing AFG formulation				Storage period, t _s			
Active type	Active conc. (% w/w)	Sample	_	1 Day	1 Week	2 Weeks	
Vanillin	0.05	VFG_0.05%		22.5% (±3.2) ^a	48.3% (±3.1) ^b	69.2% (±3.4)°	
	0.10	VFG_0.10%	E (±SD)	$28.9\% (\pm 3.2)^{a}$	25.2% (±2.9) ^a	43.9% (±3.2) ^b	
Tryptophan	0.05	TFG_0.05%		$12.3\% (\pm 3.5)^{a}$	21.4% (±3.2) ^b	33.1% (±3.7)°	
	0.10	TFG_0.10%		19.8% (±3.9) ^{a,b}	22.1% (±3.2) ^b	16.2% (±5.7) ^{a,b}	
Nicotinamide	0.05	NFG_0.05%	Ē	$0.0\% (\pm 0.0)^{a}$	$0.0\% (\pm 0.0)^{a}$	$0.0\% (\pm 0.0)^{a}$	
	0.10	NFG 0.10%		$4.1\% (\pm 1.3)^{b}$	5.6% (±1.1) ^b	$3.6\% (\pm 1.7)^{b}$	

17

18 The data shows that within the first 24 h following the production of all active-containing 19 AFG, EE was very low. Unlike typical gel particle formation approaches (e.g. emulsion 20 templating, electrostatic extrusion, spray drying) where systems are produced via the gelation 21 of a liquid precursor of comparable (to the resulting particle) dimensions (Lengyel et al., 2019), 22 fluid gel particles are formed via a nucleation and growth mechanism (Norton et al., 1999; Fernández Farrés et al., 2014). As such, the opportunity to already have an active contained 23 24 within a domain (e.g. droplet) that is then gelled, is not pertinent to fluid gels, where particle 25 formation and active entrapment would take place in tandem. With this in mind and given the 26 small molecular dimensions of all actives tested here, it is not surprising that initial EE is 27 significantly compromised.

1 However, when these systems are stored over a period of 2 weeks, the fraction of active 2 species entrapped within the fluid gel particles (still expressed as EE) increases as a function 3 of t_s , in the case of hydrophobic actives (vanillin and tryptophan). In contrast, the EE of the 4 hydrophilic active (nicotinamide) remains practically unchanged over the same period; 5 maintaining the same extremely low EE levels initially measured. Therefore, although not 6 initially encapsulated upon AFG production, both hydrophobic actives (but not the hydrophilic 7 one) migrate from the surrounding aqueous phase to the formed gel particles over the time that 8 the formulations are stored.





 $\begin{array}{c} 10 \\ 11 \end{array}$ Figure 3. Mass of actives encapsulated in AFG produced in the presence of different actives (vanillin, 12 VFG; tryptophan, TFG; and nicotinamide, NFG), as a function of active type and concentration, and 13 storage period t_s . Data are reported as mass of encapsulated active (g_a) over mass of active-containing 14 AFG formulation (g_{AFG}). All data are given as mean values ± 1 SD (error bars). Differences between 15 values (for AFG formulations containing the same type of active) marked with the same letter are not 16 statistically significant (p > 0.05).

17

18 Furthermore, the EE data reveals that this transferal takes place more efficiently (i.e. 19 resulting in a higher EE) when a lower active concentration (0.05% w/w) is used (Table 1). 20 Nonetheless, by only considering the mass of active that is entrapped into the gel particles (as 21 a function of t_s), formulations prepared at a higher active content (0.10% w/w) yield AFG 22 particles with a higher total mass of encapsulated species (Figure 3). Considering that AFG 23 particle dimensions for these formulations were shown not to be affected by the presence of 24 the active nor its concentration (Figure 2), it can be assumed that all systems would possess a comparable number of particles per unit of volume. Therefore, the data presented in Figure 3
 suggests that increasing the concentration of the active present during AFG formation results
 in particles that, over the same time period, can be loaded with a higher mass of active.

4

5 3.1.3. *Release performance*

6 Release tests for all active-containing AFG formulations as a function of active type, 7 active concentration and storage time (t_s) , were carried out under sink conditions and the results 8 are presented in Figure 4. Release testing was carried out on 'as-produced' AFG formulations, 9 without separation of the formed fluid gel particles from their continuous water phase nor dilution. Results were not adjusted to take into account the fraction of encapsulated active 10 11 within the fluid gel particles, as determined by EE analysis. As such, release data reported here 12 correspond to the cumulative release of each active (total amount of active detected in the 13 acceptor phase) and are expressed as a percentage of the active content initially used during the 14 production of all AFG formulations. Additionally, release experiments for simple aqueous 15 solutions of the actives (vanillin, tryptophan and nicotinamide aqueous solutions, denoted as 16 VAS, TAS and NAS, respectively) were carried out at a 0.10% w/w active concentration. All 17 release data were fitted to Eq. (3) and the values for the obtained model parameter n_r are 18 reported in Table 2.

19 The release curves for all fluid gel formulations follow a similar trend; an initially fast 20 release that eventually reaches a plateau, in all cases, after ~ 3 h. However, the cumulative 21 release value for this plateau varies with the type and concentration of the active as well as with 22 t_s . While the percentage of cumulative release for nicotinamide (hydrophilic) reaches 100% 23 (the full content of the active initially contained in the AFG formulation is eventually detected 24 in the release medium), the release plateau for vanillin or tryptophan (both hydrophobic) is 25 lower and is further reduced as storage time increases. It is worth noting that the release of both 26 hydrophilic and hydrophobic actives from their simple aqueous solutions also progresses to 27 their full transferal (100%) in the release medium. Furthermore, analysis of the release data 28 (Table 2) suggests that, in all cases, active transport to the acceptor phase takes place 29 predominantly by diffusion; for all systems the exponent n_r is close to 0.5 (Korsmeyer *et al.*, 30 1983).

31



3Time (h)4Time (h)5Figure 4. Cumulative release profiles under sink conditions for AFG formulations produced in the
presence of different actives; vanillin (VFG; A & B), tryptophan (TFG; C & D) and nicotinamide (NFG;
E & F). Release data for all AFG formulations are presented as a function of storage time (t_s) and active
concentration; 0.05% w/w (A, C & E) and 0.10% w/w (B, D & F). Release profiles of aqueous solutions
of vanillin (VAS), tryptophan (TAS) and nicotinamide (NAS), at a 0.10% w/w active concentration are
also shown. All data are given as mean values ± 1 SD (error bars).

- 1 **Table 2.** Model parameter n_r (mean value ± 1 SD) as a function of storage time (t_s), obtained from the
- 2 best-fit to Eq. (3) of the cumulative release data from active-containing AFG formulations shown in

3 Figure 4. Goodness-of-fit (R^2) values are also provided.

Active type	Active conc. (% w/w)	Sample	t_s	n _r	R^2
			1 day	0.58 (± 0.06)	0.99
Active type Vanillin Tryptophan Nicotinamide	0.05	VFG 0.05%	1 week	$0.56 (\pm 0.06)$	0.99
Vanillin		—	2 weeks	0.58 (± 0.09)	0.99
v ammin			1 day	$0.45 (\pm 0.08)$	0.98
	0.10	$ \begin{array}{c c c c c c c c c c c c c c c c c c c $	1 week	$0.47 (\pm 0.06)$	0.99
			$0.50 (\pm 0.04)$	0.99	
			1 day	0.55 (± 0.06)	0.99
Active type Vanillin Tryptophan Nicotinamide	0.05	TFG_0.05%	1 week	0.55 (± 0.14)	0.97
			2 weeks	$0.56 (\pm 0.06)$	0.99
пурюрнан			1 day	0.62 (± 0.06)	0.99
	0.10	TFG_0.10%	1 week	$0.60 (\pm 0.09)$	0.99
		—	$\begin{array}{c c c c c c c c c c c c c c c c c c c $	0.99	
			1 day	0.68 (± 0.14)	0.99
	0.05	NFG 0.05%	1 week	$0.66 (\pm 0.07)$	0.99
Nicotinamide		—	2 weeks	0.62 (± 0.10)	0.99
Meotinainide			1 day	0.63 (± 0.07)	0.99
	0.10	NFG_0.10%	1 week	$0.66 (\pm 0.08)$	0.99
			2 weeks	$0.67 (\pm 0.09)$	0.99

Active-containing AFG formulation

4

5 In order to better understand the effect of active type and concentration on the obtained 6 release profiles, EE data were also considered. For each AFG formulation, non-encapsulated 7 active fraction, as determined from EE data, was compared to the plateau value (cumulative 8 release percentages after 5 h) from the corresponding release profile, and results are presented 9 in Figure 5. The comparison revealed that these two quantities, regardless of the type and 10 concentration of the active and/or the period of storage, were practically the same. It is, 11 therefore, apparent that the amount of active detected during the release experiments was, in 12 all cases, the fraction of the species that was not entrapped in the first place. This further implies 13 that once an active is entrapped within the alginate fluid gel particles, then its release simply 14 does not take place, even under sink conditions. As the mass of active within the AFG particles increases with t_s , the capacity of these microstructures to retain the entrapped species is 15 16 maintained. This is obviously the case only for the systems exhibiting some level of entrapment 17 and as such this behaviour was not observed for the nicotinamide-containing AFG formulations 18 (NFG). For the latter systems release is indeed slightly delayed, in comparison to that observed 19 simply for an aqueous solution of the active, most likely as a result of the increased viscosity 20 of the AFG formulations (compared to water). Nonetheless, release does result in complete 21 expulsion of the active (100%); realised approximately after 90 minutes for NAS and 120 22 minutes for NFG.





2 NFG_0.05% NFG_0.10% 3 Figure 5. Non-encapsulated active (%) in the AFG formulations (blue) and active detected in the 4 acceptor phase after 5 h of release testing (red), as a function of active type (A: vanillin, VFG; B: 5 tryptophan, TFG; C: nicotinamide, NFG), active concentration (0.05 and 0.10% w/w) and storage time 6 t_s (1 day, 1 week, 2 weeks). All data are given as mean values \pm 1 SD (error bars). Differences between 7 values (for AFG formulations containing the same type and concentration of active) marked with the 8 same letter are not statistically significant (p > 0.05).

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10 **3.2. Effect of fluid gel particle dimensions**

11 The observation that alginate fluid gels particles appear to preferentially entrap small 12 molecular weight hydrophobic actives (but not hydrophilic ones) over a storage period of 2 13 weeks, is further explored in this section with reference to the role of AFG particle dimensions; 14 AFG particle sizes tested in the previous section were all of equivalent dimensions (~2 µm; see Figure 2). In this part, AFG formulations of two different gel particle sizes were produced in 15 16 the presence of a hydrophobic active. As the aforementioned influence was observed regardless 17 of the specific hydrophobic active and its concentration, a single active (vanillin; which 18 displayed the highest sensitivity to this effect, in comparison to tryptophan) at a single 19 concentration (0.10% w/w; the highest of those previously tested) were only considered. AFG

1 formulations were produced in the presence (and absence) of vanillin and the effect of the 2 active on AFG particle size (PSD), rheological behaviour, EE and release behaviour (under 3 sink conditions) were studied.

4

5 3.2.1. Fluid gel particle size and rheological behaviour

6 AFG formulations were produced with CaCl₂/alginate ratios of 0.125 and 0.175 (alginate 7 concentration fixed at 2% w/w and CaCl₂ concentration at 0.25 and 0.35% w/w; samples 8 VFG A and VFG B, respectively), as these fractions have been previously reported to give 9 AFG particles of distinctively different dimensions (Smaniotto et al., 2020). The two 10 CaCl₂/alginate fractions gave AFG particles with $D_{3,2}$ values of ~200 nm (ratio of 0.125) and 11 $\sim 2 \mu m$ (ratio of 0.175), regardless of whether vanillin was present (VFG) or not (AFG) during 12 their production; the particle size distributions for all fluid gel formulations are presented in 13 Figure 6. AFG particle dimensions for the lower CaCl₂/alginate ratio (0.125) were in agreement 14 to the size of alginate nano-assemblies reported by Badita et al. (2016) to form under CaCl₂ 15 and alginate contents comparable to those used here. The latter study concludes that at such 16 relatively low calcium concentrations, gelation is limited and alginate aggregates of spherical 17 shape and rough surfaces are formed with a radius of gyration of ~300 nm.

18 The shear viscosity data, together with their fit to the simple power-law model of Eq. (1), 19 for AFG formulations of both gel particle sizes, produced in the presence of vanillin or not 20 (blank), are also shown in Figure 6. The viscosity profiles for all formulations are very similar 21 and no influences, relating to the different gel particle sizes or the presence of the active, can 22 be observed. Moreover, the values for the power law fitting parameter n for all fluid gel 23 formulations suggest a similar shear thinning behaviour. Viscosity data presented here are in 24 agreement to the flow curves reported by Fernández Farrés & Norton (2014), although alginate 25 fluid gels in the latter study were formed by slowly releasing calcium from CaCO₃ using 26 glucono- δ -lactone (GDL). It is worth noting that both the PSD and shear viscosities profiles, 27 for all AFG formulations, were monitored over a period of 2 weeks, following manufacture, 28 and no significant deviation to either of these characteristics was observed.

As the concentration of vanillin used in these systems is very low, it is not surprising that the flow behaviour of the active-containing AFG formulations is equivalent to that of their 'blank' counterparts. Although, the observation that the same flow characteristics are also not affected by gel particle dimensions might appear to be an unexpected one, the reason for this relates to the microstructural attributes of these systems. The flow behaviour in the case of fluid
gels is largely dominated by the high fraction of dispersed particles typically obtained in these
formulations (reported to be close to the maximum packing fraction) and particle-specific
mechanical properties (deformability or modulus) (Garrec & Norton, 2012; Fernández Farrés *et al.*, 2014). The latter dominate FG flow behaviour at high particle fractions (higher frequency
of particle-particle contacts/interactions) and are proportional to the biopolymer concentration
(Garrec & Norton, 2012; Fernández Farrés *et al.*, 2014).

8



9 Size (μ m) Shear rate, $\dot{\gamma}$ (s⁻¹) 10 Figure 6. Particle size distributions (A) and shear viscosity curves (B) for alginate fluid gels, formed in 11 the absence (AFG; *blank*) and the presence of vanillin (VFG), as a function of the used CaCl₂/alginate 12 ratio; 0.125 (AFG_A and VFG_A) and 0.175 (AFG_B and VFG_B). All data are given as mean values 13 ± 1 SD (error bars).

14

15 The influence of particle deformability on the flow behaviour of fluid gels or high phase volume suspensions of microgel particles, has also been reported in whey protein fluid gels 16 (Moakes et al., 2015) and (high phase volume suspensions of) a range of agar microgel particles 17 18 (Adams et al., 2004). Although, none of the fluid gel formulations studied here were diluted 19 (i.e. they should all possess a high gel particle phase fraction) and all were formed using the 20 same alginate concentration (2% w/w), the calcium content of the VFG A (or AFG A) fluid 21 gel nano-particles and the VFG B (or AFG B) fluid gel micro-particles are different. Albeit at slightly higher concentrations to those studied here, Fernández Farrés & Norton (2014) 22 reported that increasing the calcium content leads to an enhanced AFG particle stiffness. 23 24 However, Moakes et al. (2015) suggest that deformability is also a function of size, with larger

1 particles being easier to deform compared to the more rigid smaller ones. It is not clear whether 2 either of these contrasting effects apply to the low calcium concentrations and/or the small gel 3 particle dimensions investigated here. It might be that both these arguments do apply and 4 eventually cancel each other out; i.e. the alginate micro-particles, produced at the higher 5 calcium concentration, are indeed stiffer than the alginate nano-particles, but at the same time 6 the former are more deformable than the latter due to their larger dimensions. Whatever the 7 case, it is evident that the flow behaviour of these systems is greatly affected by the large 8 particle phase volumes typically encountered in fluid gel formulations, an effect that appears to dwarf any other influences. 9

10

11 3.2.2. Encapsulation efficiency

12 The data on the EE for all vanillin-containing AFG formulations as a function of fluid 13 gel particle size are reported in Table 3; note that formulations corresponding to samples 14 VFG B (Table 3) and VFG 0.10% (see Table 1) are the same. Regardless of particle size, 15 both VFG A and VFG B fluid gel formulations exhibit an EE enhancement with increasing storage time t_s . This trend of increasing EE under storage is similar to what was earlier shown 16 17 for AFG formulations containing either 0.05% or 0.10% w/w of vanillin or tryptophan (Table 18 1). Nonetheless, the rate and magnitude of the EE increase (of the same active) observed in this 19 case, appear to be significantly influenced by the dimensions of the AFG particles.

20 More specifically, the EE increase for the VFG A formulation appears to progress more 21 rapidly and reaches a higher value than that for VFG B. As vanillin is much smaller (radius of 22 gyration of ~ 0.47 nm; Yaws & Leh, 2009) than the reported average pore size of the alginate 23 gel network (~ 5 nm; Lee & Mooney, 2012), it can be assumed that the observed migration of 24 this active, from the bulk aqueous phase of the fluid gel formulations to the interior of the fluid 25 gel particles, should take place predominantly by diffusion. In this case, Fick's second law 26 would be sufficient to describe this process. As such diffusion of vanillin would be expected 27 to depend on three parameters: the active's concentration difference between the exterior and 28 the interior of the particle, the diffusion coefficient or diffusivity of the particle structure and 29 the diffusion length or path (Li & Mooney, 2016). As the vanillin concentration used and the 30 initial EEs for the VFG A and VFG B formulations are more or less the same (Table 3), a 31 similar concentration differential (between bulk aqueous phase and AFG particles) driving 32 diffusive migration is expected. However, although particles in both systems would consist of 33 similar 'building blocks' (i.e. assemblies of alginate polymer chains), the presence of a higher

1 Ca²⁺ concentration in the VFG B system would suggest the presence of an alginate network 2 with a higher degree of cross-linking; and thus lower diffusivity, as suggested by literature (Lee 3 & Mooney, 2012). What is more, the diffusion path for vanillin to be transported into the 4 AFG A fluid gel particles is significantly shorter than that in the case of AFG B, because of 5 the difference in their dimensions. In conclusion, the observed variance in the amount of 6 vanillin that is accumulated in the VFG A over the VFG B AFG particles during the studied 7 storage period, can be explained primarily due to the much smaller sizes of the former 8 (VFG A) and also because of the reduced diffusivity of the polymer network in the latter 9 (VFG B).

10

11 **Table 3.** Encapsulation efficiency (EE; mean value ± 1 SD) of vanillin-containing AFG formulations

12 as a function of gel particle size $(D_{3,2})$ and storage time (t_s) . Differences between EE values (for the

13 same active) marked with the same superscripted letter are not statistically significant (p > 0.05).

Vanillin-containing AFG formulation			-	Storage time, <i>t</i> s			
	CaCl ₂ /ALG ratio	$D_{3,2}(\mu m)$	Sample		1 Day	1 Week	2 Weeks
	0.125	0.15	VFG_A	±SD)	24.2% (±2.5) ^a	49.5% (±3.3) ^b	73.3% (±2.9)°
	0.175	1.90	VFG_B	EE (=	28.9% (±3.2) ^a	25.2% (±2.9) ^a	43.9% (±3.2) ^b

14

15 3.2.3. *Release behaviour*

Release testing for vanillin-containing AFG formulations as a function of FG particle 16 17 size and storage time (t_s) , were carried out under sink conditions and the results are presented 18 in Figure 7. Release data were fitted to Eq. (3) and the obtained model parameter n_r is reported 19 in Table 4. The shape of the release curves is similar to that exhibited by all other active-20 containing AFG formulations discussed previously (see Figure 4); an initial fast discharge that 21 progresses over time to reach a plateau in terms of cumulative release. The value for this 22 plateau, earlier shown to vary with the type and concentration of the active, is in addition 23 revealed here to be affected by AFG particle size, while the strong dependency on t_s is retained. 24 Although a final cumulative release of approximately 75% (w/w) of the initial vanillin content 25 (same for both AFG formulations) is detected 1 day following their formation, this is ultimately suppressed (upon increasing the storage period to 2 weeks) to 30% and 58% (w/w) for the AFG 26 27 nano-particles (VFG A) and micro-particles (VFG B), respectively (Figure 7). However, 28 regardless of AFG particle dimensions or storage period, analysis of the data in Figure 7 29 suggests that vanillin release takes place predominantly by diffusion ($t_r \approx 0.5$; Table 4).

1 What is more, for both the VFG A and VFG B AFG formulations, the non-encapsulated 2 vanillin fraction, as determined from the EE analysis (Table 3), and the maximum vanillin 3 cumulative release, as detected in the aqueous acceptor phase after 5 h, are practically identical 4 (Figure 8). Therefore, as discussed earlier, the amount of vanillin that is released from the AFG 5 formulations, despite changes to the fluid gel particle size, corresponds to the fraction of active 6 that was not entrapped. As such, the previously established capacity of the fluid gel particles 7 to fully retain (under sink conditions) their enclosed hydrophobic species regardless of the 8 active concentration used, is shown here to further persist irrespective of the dimensions of the 9 AFG particles themselves.

10



11 12

12 Figure 7. Vanillin cumulative release from vanillin-containing AFG (VFG) formulations of different

- 13 gel particle sizes, produced at CaCl₂/alginate ratios of 0.125 (VFG_A; AFG nano-particles) and 0.175 14 (VFG B; AFG micro-particles), as a function of storage time (t_s). All data are given as mean values
- 15 ± 1 SD (error bars).

16

- 17 **Table 4.** Model parameter n_r (mean value ± 1 SD) obtained from the best-fit to Eq. (3) of the cumulative
- 18 release data from the vanillin-containing AFG (VFG) formulations (Figure 7), as a function of gel
- 19 particle size $(D_{3,2})$ and storage time (t_s) . Goodness-of-fit (R^2) values are also provided.

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CaCl ₂ /ALG ratio	$D_{3,2}(\mu m)$	Sample	t_s	<i>n</i> _r	R^2
			1 day	$0.54 (\pm 0.05)$	0.99
0.125	0.15	VFG_A	1 week	$0.49 (\pm 0.08)$	0.98
			2 weeks	0.51 (± 0.04)	0.99
			1 day	$0.45 (\pm 0.08)$	0.98
0.175	1.90	VFG_B	1 week	$0.47 (\pm 0.06)$	0.99
			2 weeks	$0.50 (\pm 0.04)$	0.99

Vanillin-containing AFG formulation



Figure 8. Non-encapsulated active (%) in the vanillin-containing AFG formulations (blue) and active detected in the acceptor phase after 5 h of release testing (red), as a function of AFG particle size and storage time t_s (1 day, 1 week, 2 weeks). FG formulations produced at CaCl₂/alginate ratios of 0.125 (VFG_A; fluid gel nano-particles) and 0.175 (VFG_B; fluid gel micro-particles). All data are given as mean values \pm 1 SD (error bars). Differences between values (for the same vanillin-containing AFG formulations; VFG_A or VFG_B) marked with the same letter are not statistically significant (p > 0.05).

8

9 **3.3.** Proposed mechanism for the encapsulation and release behaviour of small

10 molecular weight hydrophobic actives in alginate fluid gels

It is proposed here that the migration of small molecular weight hydrophobic actives (vanillin, tryptophan) to the interior of the AFG particles occurs via diffusion and storage of these systems post production and over a period of 2 weeks, leads to significant increases in active loading/encapsulation. Moreover, release (under sink conditions) from the AFG formulations is only limited to the fraction of the active that is not entrapped within the gel particles. This overall behaviour in terms of the encapsulation and release of small molecular weight hydrophobic actives in AFG is schematically presented in Figure 9.

Based on Fick's second law, it is suggested that the diffusional loading of the hydrophobic actives within the fluid gel particles will depend on the active's concentration difference between the exterior and the interior of the particle, the diffusion coefficient of the particle structure and diffusion length (Li & Mooney, 2016). These influences were discussed earlier to explain the variation in the rate and magnitude of loading exhibited by AFG particles of different dimensions; AFG nano- (VFG_A) and micro-particles (VFG_B) (Table 3). Nonetheless, the rate of loading observed here is much lower than that reported for other

1 hydrophobic actives within alginate gel particles. Tanaka et al. (1984) studied the diffusion of 2 several species of different molecular weights, both into and from calcium-alginate gel beads, 3 and reported that an equilibrium concentration of tryptophan in the particles was obtained after 4 only 30 min of placing blank beads into an aqueous buffer solution of the active. Tu et al. 5 (2005) prepared alginate microparticles by a spray-coagulation method and studied the loading 6 and release of 4-phenylazoaniline (PAA). Active loading was carried out by suspending the 7 blank alginate particles (110 - 212 µm), in an ethanol solution of PAA for a 24 h period. 8 Although, PAA loading efficiency was not reported it is suggested that the duration of the used 9 loading stage was sufficient to induce the highest possible level of active inclusion into the 10 particles. Elsewhere, Hariyadi et al. (2010) studied the diffusional loading and release of 11 ibuprofen within alginate gel microparticles produced via an impinging aerosols method. In 12 this case, an aqueous suspension of alginate gel microparticles was added to an ibuprofen water 13 solution and stored at room temperature for 24 h; ibuprofen loading was within the range of 23-29% w/w. 14

15 In the present study, active loading takes place within 'intact' AFG formulations; i.e. 16 AFG particles were not separated from their continuous aqueous medium and the formulation 17 was not diluted. Therefore, although the diffusion coefficient of the particle structure can be 18 assumed to be the rate-limiting step for active loading in other studies (and expected to be 19 comparable to that observed for the AFG particles here), what appears to primarily govern the 20 incorporation of the actives within the formulations studied here is the rate of diffusion through 21 the continuous phase; i.e. the rate by which actives can diffuse to the surface of the AFG 22 particles for entrapment to take place. This is not necessarily expected to directly relate to the 23 much higher bulk viscosity of the AFG formulations (compared to that of water). In addition 24 to this what should also be taken into account is the significant impact to the diffusion path of 25 the active from the presence of a very high fraction of dispersed particles; even though the 26 continuous medium surrounding these particles can be assumed to possess a 'local' viscosity 27 that approaches that of water. In many ways, this phenomenon is equivalent to what has been 28 termed a "cage effect" in suspensions of hard-sphere-like colloidal particles at high fractions 29 $(\phi > 0.52)$. (Kasper *et al.*, 1998).

The data in the current work suggest that, once the hydrophobic actives diffuse to the AFG particles, they are eventually incorporated within the particle structure. Paradoxically, this was not observed for hydrophilic actives. This is despite the fact that both alginate quiescent gels and alginate gel particles are overwhelmingly regarded in literature as ideal

1 structures for the enclosure of hydrophilic species (e.g. Josef et al., 2010). Release experiments 2 carried out for vanillin-containing AFG were replicated for simple aqueous solutions of the active (0.10% w/w) in the presence of alginate (2% w/w), but without the addition of calcium; 3 i.e. no alginate gel formation (Figure 10). It is evident that, regardless of the storage time 4 5 imposed, alginate alone only slightly delays the release rate of vanillin (compared to that from 6 a simple vanillin aqueous solution) and in all cases the active is fully discharged into the 7 acceptor phase after 2-3 h. Therefore, the retention of vanillin observed earlier (see Figure 4 8 and Figure 7) appears to be directly related to the existence of the alginate gel network.







Figure 9. Schematic representation of the loading/encapsulation and release behaviour of small
 molecular weight hydrophobic actives in AFG particles.

13

Despite the entropic penalty relating to disproportionately placing vanillin in the water phase associated with the AFG particles (in comparison to the aqueous continuous phase), this migration does take place and should therefore provide an enthalpic advantage. It has been

1 previously shown that the addition of small amounts of alcohol (ethanol) decreases the aqueous 2 solubility of vanillin due to the reinforcement of water structuring, whereas higher alcohol 3 concentrations increase vanillin solubility as a result of water structure disruption (Kappatos et al.,1996). Probst et al (1985) showed that Ca^{2+} , due to its size and strength of the ion-water 4 5 interaction, is also able to disrupt the structure of the water quite effectively. It is therefore 6 proposed that the presence of calcium could facilitate an enhancement to the capacity of water 7 to solubilise vanillin. As calcium is predominantly associated with the alginate gel matrix, any 8 such improvement in the solvent quality of water would be localised; primarily confined to 9 water situated within the gel porous structure. Such a difference in vanillin solubility would 10 indeed offer a significant enthalpic incentive for the migration of the active into the alginate 11 gel matrix.

12



Figure 10. Vanillin cumulative release from a vanillin (0.10% w/w) aqueous solution (VAS) and vanillin (0.10% w/w) aqueous solutions also containing alginate (VAN-ALG), the latter as a function of storage time (t_s). All data are given as mean values ± 1 SD (error bars).

17

The hypothesis outlined above would also be relevant to explain why active entrapment persists even when the AFG formulations are placed within an aqueous sink; the release of the encapsulated fraction of the hydrophobic species is hindered. In addition to solvent-specific enthalpic contributions to the retainment of vanillin (or tryptophan) within the AFG particles, what should also be considered is the influence(s) of interactions between the hydrophobic actives and alginate and/or calcium in the gel matrix. Vanillin has been reported to interact

1 with amino acids and proteins via Schiff base formation (covalent binding of the aldehydic 2 function of vanillin to the amino groups of proteins), hydrogen bonding, hydrophobic and 3 electrostatic interactions (Weerawatanakorn et al., 2015). It has been shown that vanillin can 4 interact with a range of proteins, including β -lactoglobulin, sodium caseinate, bovine serum 5 albumin, ovalbumin, whey, milk, soy and pea protein (Chobpattana et al., 2002; Houde et al., 6 2018; Wang et al., 2011; Weerawatanakorn et al., 2015). Mikheeva et al. (1998) reported that 7 vanillin can interact with β-lactoglobulin, bovine serum albumin, and ovalbumin through 8 electrostatic interactions. Chobpattana et al. (2002) showed that hydrophobic interactions are 9 the main forces between vanillin and bovine serum albumin, while the interactions between 10 vanillin and casein or sodium caseinate are primarily driven by hydrogen bonding. Finally, 11 interactions between calcium and the quadrupole moment of the aromatic ring in vanillin or 12 tryptophan (cation- π interactions) could also become important (Mahadevi & Sastry, 2013). 13 Although, the data in Figure 10 could be interpreted to suggest that the influence of any such 14 interactions between vanillin and the alginate chains on the release kinetics of the active is 15 minimal to practically non-existent, this might not be the case within an AFG particle setting. 16 Considering events taking place within any single pore of the AFG particle network, the 17 plurality and proximity of functional sites/groups would enhance the probability of such 18 interactions taking place, and thus could impact on the retention of the actives in question.

19

20 4. Conclusions

Although the encapsulation of active components in gelled microparticles is generating great interest, the scalable production of such systems still remains challenging. Fluid gels are a class of soft-solid gel particles that can be produced via high-shear approaches that fully align with industrial manufacture. As such, there is a (currently unmet in open literature) need to study fluid gel formulations for their capacity to entrap actives.

26 In this work, the encapsulation of vanillin and tryptophan, as hydrophobic small 27 molecular weight model actives, and nicotinamide, as a hydrophilic one, in cross-linked 28 alginate fluid gel (AFG) particles has been investigated. It was demonstrated that the presence 29 of an active does not affect the dimensions of the AFG particles (maintaining a mean diameter, 30 $\overline{D}_{3,2}$, of 1.91±0.12 µm) nor their bulk rheological properties (a shear thinning behaviour with 31 an average power law index , n, of 0.32 ± 0.02). The encapsulation efficiency of all small 32 molecular weight actives in the AFG particles is initially (after 1 day of storage) extremely low 33 (<30%), since both active entrapment and particle formation take place in tandem. However,

1 hydrophobic actives were shown to migrate into the AFG particles post formation and over a 2 storage period of 2 weeks; with EE values of up to 70% (in the case of vanillin) at the end of 3 the storage period. It is proposed that the calcium ions, located within the alginate gel network, 4 disrupt the structure of water present therein, thus enhancing the aqueous solubility of the 5 hydrophobic species. By essentially confining this enhancement to the water's solvent quality 6 within the AFG particles, an enthalpic advantage that encourages the migration of the 7 hydrophobic species, from the continuous aqueous medium to the water located within the 8 alginate gel matrix, is created. The rate of the migration of the hydrophobic actives seen here 9 is much lower than that typically observed during the diffusional loading of hydrophobic 10 actives into alginate gel microparticles. The reason for this delayed loading is the much greater bulk viscosity of the medium over which diffusion takes place as well as the significantly 11 12 increased diffusion path for a small molecular weight active within an aqueous phase containing a high fraction of closely packed gel particles. The rate and magnitude of the 13 14 incorporation of the hydrophobic actives within the alginate fluid gel particles is however 15 accelerated by increasing the concentration of the species initially added in the formulation or 16 by decreasing the size of the gel particles; EE values for vanillin entrapment in AFG nano-17 (VFG A) and micro-particle (VFG B) systems were 73.3% and 43.9%, respectively. Thus, 18 both the initially imposed concentration difference of the active between the suspending 19 aqueous medium and the interior of the AFG particles as well as and diffusion path within the 20 particles' gel network, also seem to impact upon the hydrophobic species' loading rate and 21 loading extent. Release under sink conditions revealed that encapsulated hydrophobic content 22 is essentially confined within the fluid gel particles and only the non-encapsulated fraction of 23 the species is detected in the acceptor phase. It is argued that in addition to the enhanced solvent 24 quality of water in the interior of the particles, the occurrence of a number of interactions that 25 have been previously reported to occur between these or similar hydrophobic compounds and 26 hydrocolloids and/or calcium, exaggerated by the proximity and plurality of these species 27 within each pore of the gel network, could also impact on the retention of the actives. Future 28 efforts would obviously need to focus on studying the release of such hydrophobic species 29 (from AFG formulations) in simulated gastric and intestinal media.

The present findings show clear evidence that AFG can be preferentially loaded with small molecular weight hydrophobic species and the hypotheses reported here for the first time, offer insight that is valuable to future efforts into achieving control over these phenomena. Regulating the loading/encapsulation and release of actives from AFG will significantly

- intensify the applicability of these formulations, a class of colloidal systems with demonstrated 1
- 2 potential in terms of industrial manufacture.
- 3

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